

The present invention relates to a heat-sensitive chemical composition comprising a hydrophobic organic solvent, an "organogelling" substance and a bioactive substance, the said composition being intended to be administered to a living organism, for the sustained delivery of bioactive substances.

5       The said composition has the capacity to form an organogel spontaneously or by cooling, once placed in contact with an aqueous medium, and especially a physiological fluid. The said organogel formed serves as a support for the sustained release of bioactive substances by diffusion and/or erosion and/or gradual biodegradation of the said organogel in the body.

10       The present invention also covers the uses that may be made of this composition in the therapeutic field and more particularly in the field of the sustained delivery of bioactive substances.

      The expression "heat-sensitive composition" means any composition capable of changing from the liquid state to the gel state as a function of the  
15       temperature, and the term "organogel" means any gel whose liquid phase is composed of an organic solvent.

      Moreover, the expression "bioactive substance" means any substance that has the capacity to act on a living organism or its functioning so as to prevent, cure, relieve or improve the condition of the said organism.

20       The expression "hydrophobic organic liquid" means an organic solvent or a mixture of organic solvents whose molecules or parts of molecules have a certain level of repulsion towards water molecules. The expression "hydrophilic solvent" means a solvent whose molecules establish attraction interactions with water molecules.

25       Gels have been used for a long time in the industrial field for the properties imparted to them by their particular physical structure.

      Specifically, they correspond to an intermediate state of matter since they are composed both of elements in solid form and of elements in liquid form. The solid elements form a three-dimensional structure or matrix, organized as a  
30       network of mutually interconnected molecules, this network immobilizing the elements present in liquid form.

      Gels may be classified as a function of the type of bonds that link

together the molecules of the solid phase, or as a function of the type of organic or aqueous solvent of which the liquid phase is composed.

"Hydrogels" are gels whose liquid phase is an aqueous phase, to distinguish them from "organogels" whose liquid phase is an organic phase.

5           Gels whose matrix consists of molecules linked together via covalent bonds are generally in a stable and irreversible state once formed. In contrast, gels whose solid matrix is obtained by bonds of low energy (such as hydrogen bonds or Van der Waals bonds especially) are generally reversible gels, i.e. they can change from the gel state to the liquid state as a function of the  
10           surrounding conditions (pH, temperature, ionic strength, etc.).

          In the case of heat-sensitive gels, the temperature at which the change of state is observed is known as the transition temperature. In the particular case of systems showing hysteretic behaviour, the gel/liquid transition temperature is different from the liquid/gel transition temperature.

15           Thus, gels are especially used in the pharmaceutical industry for their retention capacity with respect to bioactive molecules, especially in the context of a transcutaneous administration of active substances.

          This retention property has moreover been exploited for a use of gels as vehicles for the sustained delivery of medicinal products.

20           Thus, patent US 3 932 624 describes the use of a hydrogel intended for the delayed delivery of saralazine. In the said patent, the gel is prepared based on gelatin, which, diluted in a physiological saline solution containing the bioactive substance, becomes impregnated therewith to form a gelled structure that may be surgically implanted into the body subcutaneously. The implanted  
25           gel gradually releases the active substance it contains by gradual erosion of the said gel.

          However, this type of use necessitates the *in situ* surgical implantation of a preformed gel. This operation thus remains both expensive and a limitation on the patient.

30           To overcome this drawback, hydrogels that form *in situ* have been developed. Thus, recently, patent application US No. 20010007673 describes

the use of an *in vivo*-formed hydrogel intended to the delayed delivery of bioactive molecules, especially proteins. A composition based on hydrophilic polymer including alginate, on a polyvalent metal ion and on the desired active substance is injected in liquid form and changes to gel form once placed into  
5 the body. In addition, due to the thixotropic nature of the composition in the gel state, the composition can be injected while in the state gel, e.g. by pressure from the syringe, where upon the composition can regel in the body. This hydrogel allows a delayed diffusion of the bioactive substance into the bodily fluids.

10 Moreover, patent US 5 575 815 describes the intracavitary administration of an aqueous liquid composition that is converted or viscosified into a hydrogel *in vivo*. The use of this gel for the incorporation of active substances is envisaged especially for angioplasty. The hydrogels used consist of polyether polymers.

15 Patent US 6 344 488 describes a temperature-controlled pH-dependent gel comprising chitosan/organo-phosphate aqueous mixture. The addition of mono-phosphate dibasic salt of polyol or sugar to chitosan aqueous solutions leads to temperature-controlled pH-dependent gelation. Drugs are incorporated within said gel prior to the gelation. Chitosan/organo-phosphate mixtures are  
20 stored at low temperatures in the solution state, and gel in situ following subcutaneous, intraperitoneal or intramuscularly injection. This hydrogel can be used for the delivery of pharmacologically active compounds.

Patent application WO 97/15287 describes a system and method for the parenteral delivery (e.g. intramuscular, intraperitoneal, subcutaneous) of a drug  
25 in a biodegradable polymeric matrix to a warm blooded animal as a liquid with the resultant formation of a gel depot for the controlled release of drug. The liquid is an aqueous solution having dissolved or dispersed therein an effective amount of drug contained in a biodegradable block copolymer matrix. The copolymer has a reverse gelation temperature below the body temperature of  
30 the animal to which it is administered and is made up of hydrophobic polymer block and hydrophilic polymer block.

Other thermogelling aqueous solutions have been described in the literature. Among them one can cite poloxamer (Johnston, T.P. et al., Inulin disposition following intramuscular administration of an inulin/poloxamer gel matrix, J. Parent. Sci. Technol., vol. 43, 279, 1989; Johnston, T.P. et al.,  
5 Sustained delivery of interleukin-2 from a poloxamer 407 gel matrix following intraperitoneal injection in mice, Pharm. Res. 9, 425, 1992; Pec et al., Biological activity of urease formulated in poloxamer 407 after intraperitoneal injection in the rat, J. Pharm. Sci. Vol.81, 626, 1992) and xyloglucan (Miyazaki, S. et al., Thermally reversible xyloglucan gels as vehicles for rectal drug delivery, J.  
10 Controlled Release, vol 56, 75, 1998).

However, the main drawback of these hydrogels lies in their relative poor efficacy in terms of delivery of hydrophilic bioactive substances and especially those having a low molecular weight over long periods of time. This is due especially to their high proportion of water which gives them a high level of  
15 porosity, leading the hydrophilic bioactive substances present in such gels to be released relatively quickly. This phenomenon of diffusion is particularly important for very hydrophilic molecules of small size, for example such as certain hydrophilic medicinal products or certain hydrophilic peptides. The efficacy of the sustained release of these substances is therefore consequently  
20 reduced.

The object of the present invention is to provide a novel pharmaceutical composition that has the capacity to form an organogel allowing the release of active substances over long periods of time.

Furthermore, the object of the present invention is also to provide such a  
25 delayed-release support that is both biocompatible and biodegradable, also allowing it to be administered in liquid form, i.e. easily, quickly and inexpensively.

Organogels have already been used as a support for the delayed release of active principle.

30 The present invention relates to a hydrophobic organogel generated in vivo after being applied under liquid form. Such gels have already been

described in the prior art.

Patent application No. WO 94/08623 discloses a hydrophobic organogel containing lecithin and a hydrophobic solvent for lecithin, which is used for the delayed release of proteins. The gel forms *in vivo*, using a solution injected  
5 intramuscularly or subcutaneously, by absorption of water from the interstitial medium during injection.

In contrast, the hydrophobic organogel of the present invention is not formed by absorption of the surrounding water.

The present invention relates to a heat sensitive liquid composition with  
10 gelling properties comprising a hydrophobic organic liquid, an "organogelling" substance and a bioactive substance.

The organogelling substance consists of molecules capable of binding together via bonds of low energy to the extent that the self-assembly of these molecules is advantageously heat-reversible.

15 The heat-sensitive composition in liquid form according to the invention contains a hydrophobic organic liquid, an organogelling substance, the molecules of which have the capacity to bind together via bonds of low energy, and a bioactive substance. It changes to the organogel form when it comes into contact with a physiological fluid, during its administration into an animal body,  
20 in particular man, in particular during injection into the body, for example using a conventional syringe, via the extravascular parenteral route.

The expression "extravascular parenteral route" means any route of penetration into the body other than the digestive route and the vascular route (veins, arteries and blood vessels).

25 The composition of the invention may also be administered intraocularly, intracavitally or on prostheses prior to their application, vaginally, to an open wound or during surgery.

Many documents describe topical-use compositions containing lecithin-based organogels (see, for example, US 6 306 383). Lecithin is a mixture of  
30 phospholipids of low molecular weight. Lecithins are amphoteric, soluble in alcohol and form an emulsion with water. Lecithin organogels have been

described as vehicles that are useful for facilitating the penetration of low molecular weight molecules (H. Willmann, et al., -Lecithin organogel as a matrix for the transdermal transport of medicinal products, J. Pharm. Sci., vol. 81, 871, 1992). Lecithin organogels are obtained by adding a small amount of  
5 water to a solution of lecithin in organic solvents such as isopropyl palmitate or cyclooctane. In these documents, the water is added to form the desired gel so that the organogel is formed before it is applied to the skin.

In contrast, the organogels of the present invention are in liquid form when they are administered to a living organism, and take the form of a gel  
10 once they come into contact with a physiological fluid. Moreover, lecithins do not constitute organogelling substances as defined in the context of the present invention.

The expression "physiological fluid" means any fluid circulating in an animal body such as, for example, lymphatic fluid, lacrymal fluid, cerebrospinal  
15 fluid, amniotic fluid, parenteral fluid and blood.

The organogel formed from the composition according to the invention has capacities for retaining bioactive molecules and more particularly molecules less than 100 000 daltons in weight and of hydrophilic nature, enabling a release of the said molecules into the body over periods longer than 3 days to  
20 be envisaged.

Finally, the said organogel formed in the body from the composition according to the invention has the capacity to be eliminated slowly by gradual erosion and/or biodegradation, without toxicity to the body in which it is  
implanted.

25 This property of *in situ* gelation in accordance with the invention is obtained by using a hydrophobic organic liquid, constituting the organic phase of the said organogel, and via an organogelling substance, constituting the solid matrix of the said organogel.

The molecules constituting this organogelling substance are especially of  
30 the type such as fatty acid ester derivatives of amino acids, which have the capacity to self-assemble spontaneously to form a matrix that immobilizes the

said hydrophobic organic liquid. This molecular self-assembly may be achieved by hydrogen bonds that become established between the groups of alcohol (-OH), acid (-COOH) and amine (-NH or NH<sub>2</sub>) type borne by the organogelling molecules.

- 5           If necessary, the gelation of the liquid composition is induced by cooling the site of application of the composition or by diffusion of a hydrophilic organic solvent added to the composition of the invention.

          The Applicant has selected hydrophilic organic solvents capable of creating weak bonds (e.g.: hydrogen bridges) with the molecules of  
10   organogelling substance, and capable of diffusing into aqueous media to produce the composition according to the invention.

          Thus, the hydrophilic organic solvent introduced into the mixture forming the composition according to the invention will come into competition with the molecules of organogelling substance, creating with the said molecules weak  
15   bonds (e.g.: hydrogen bridges) that prevent the said molecules from self-assembling into a unified network. The composition according to the invention will thus remain in liquid form for as long as the molecules of the said hydrophilic organic solvent remain bound to the organogelling molecules.

          The use according to the present invention of the reversibility of the weak  
20   bonds will advantageously allow the organogelling matrix to become reassembled as soon as the said hydrophilic organic solvent has diffused into the surrounding medium.

          Thus, as soon as it comes into contact with an aqueous solution and more particularly with physiological fluids such as interstitial fluid, lymph or  
25   intraperitoneal fluid, for example, the said hydrophilic organic solvent present in the composition in accordance with the invention will diffuse into the said surrounding fluid due to its hydrophilicity.

          The diffusion of the said hydrophilic organic solvent will then allow the molecules of the said organogelling substance to self-assemble. By creating a  
30   structured network, this self-assembly will allow the said hydrophobic organic liquid to be retained, causing the said composition to change from the liquid

state to the gel state.

The present invention thus offers a simple system for spontaneous *in situ* gelation and easy administration.

Moreover, the present invention is based on the hysteretic properties  
5 observed by the Applicant on organogels based on organogelling substances in  
accordance with the invention. The term "hysteresis" means the physical  
phenomenon observed especially for gellable compositions, representing the  
difference existing between the gel/liquid transition temperature and the  
liquid/gel transition temperature. Specifically, with these properties, a  
10 composition in accordance with the invention that is liquid, and thus readily  
injectable, at room temperature (or at a temperature in the region of room  
temperature) may be envisaged. Furthermore, with these properties, an  
organogel according to the invention may also be produced, which, once  
formed *in vivo*, will remain in gel form at the body temperature of the organism  
15 under consideration. The reason for this is that such an organogel, whether it is  
formed by diffusion or by simple cooling, has a gel/liquid transition temperature  
that is higher than the temperature of the site of injection or of application.  
Consequently, it is entirely stable in the said organism.

Finally, the present invention has the advantage of providing a support  
20 for the sustained release of medicinal products or other active substances.  
Specifically, the organogel formed in the organism and in accordance with the  
present invention comprises a veritable organized matrix structure that has little  
affinity for the surrounding aqueous medium, and thus allows a slow release of  
the active substance by gradual diffusion, erosion or biodegradation of the said  
25 organogel.

The present invention thus provides a simple, effective and easily  
administered support for sustained release into the body, over a period at least  
equal to 1 day, of substances such as bioactive substances and more  
particularly of molecules of hydrophilic nature weighing less than  
30 100 000 daltons.

In addition, the composition according to the present invention has the



advantage of being extremely inexpensive, both in terms of manufacture as is described later, and in terms of packaging and administration.

The organogelling substances in accordance with the invention are substances whose molecules have the capacity to bind together via bonds of  
5 low energy, and especially via hydrogen bonds, allowing the formation of a heat-sensitive matrix. These molecules are especially molecules of low molecular weight with acid (-COOH) or alcohol (-OH) or amine (-NH<sub>2</sub> or -NH) end groups, for example.

Moreover, these substances are preferentially biocompatible and do not  
10 give rise to metabolites that are toxic or hazardous to the body during their degradation by the said body.

Derivatives of amino acids or fatty acid ester derivatives of amino acids such as alanine, which not only display good biocompatibility and satisfactory organogelling power, but also mainly give the gelled system hysteretic  
15 properties, will preferably be used. These properties are reflected by a change from the liquid state to the gel state at a different temperature from that observed during the change from the gel form to the liquid form of the said composition. The Applicant has, to its credit, noted that the difference between these two transition temperatures varies as a function of the type of  
20 hydrophobic organic liquid used, and of the amount of organogelling substance used.

Thus, the Applicant has produced compositions in accordance with the invention whose transition temperatures and differences between these temperatures may be adjusted by simple modification of these two parameters.  
25 The results reflecting these variations are shown in Figures 1 to 7.

Preferably, the difference between these two transition temperatures is chosen such that the liquid/gel transition temperature is less than the body temperature of the living organism under consideration, in particular in the case where the organogel is administered without a hydrophilic organic solvent, and  
30 such that the gel/liquid transition temperature is higher than the abovementioned temperature.

Thus, alanine derivatives such as N-lauroyl-L-alanine acid (LA) or alanine derivated esters such as N-lauroyl-L-alanine methyl ester (LAM) , N-Lauroyl-L-alanine ethyl ester (LAE), N-stearoyl-L-alanine methyl ester (SAM), or N-stearoyl-L-alanine ethyl ester (SAE) will preferably be used as the organogelling  
5 substance in accordance with the invention.

The amount of organogelling substance depends on the type of hydrophobic organic solvent used and on the transition temperature that it is desired to select for the organogel in accordance with the invention.

However, the proportion of this substance is advantageously chosen  
10 between 0.5 and 50% by weight relative to the total weight of the said composition.

The Applicant has found that the use as an organogelling substance of N-lauroyl-L-alanine methyl ester allows the said composition to change to the gelled state by simple cooling below the liquid/gel transition threshold and to  
15 remain in the gel state at a temperature above the liquid/gel transition temperature, in particular the temperature of the living organism.

Specifically, the Applicant has noted that the said organogel formed by cooling is stable in the range of temperatures between the liquid/gel transition temperature and the gel/liquid transition temperature.

20 This combination of observations led the Applicant to develop a heat-sensitive composition with gelling properties that have the capacity to change to gelled form by simple local cooling and to maintain this gelled state at the body temperature. In this particular case of the invention, the amount of hydrophilic organic solvent may be extremely small, or even zero since the gelation takes  
25 place by cooling the said composition rather than by diffusing the said hydrophilic organic solvent.

This embodiment is particularly advantageous since the presence of the hydrophilic organic solvent can be dispensed with, and thus the process for preparing the composition according to the invention can be further simplified  
30 and its cost price can also be reduced.

Thus, according to one particular embodiment, the heat-sensitive

composition according to the invention contains a proportion of N-lauroyl-L-alanine methyl ester that is sufficient to allow the said composition to change from the liquid state to the organogel state by simple cooling of the said composition on contact with its site of injection into the body.

5           Such a cooling must be sufficient to cause the said composition, applied in liquid form, to change to its gelled form. This cooling, which may be performed by external application of a cold object such as an ice pack or a cold compress or any other cooling means around the site of injection, must allow a local cooling, to below the liquid/gel transition temperature of the said  
10 composition.

          The composition according to the invention is thus preferably in liquid form at the temperature of the site of application, has a gel/liquid transition temperature that is higher than the body temperature and a liquid/gel transition temperature that is lower than the temperature of the organism under  
15 consideration or of the area into which the gel is implanted. Specifically, the skin temperature may be a few degrees lower than the general temperature of the organism.

          In one preferred embodiment, the proportion of N-lauroyl-L-alanine methyl ester in the said composition is sufficient for the liquid/gel transition  
20 temperature to be below body temperature (37°C in general) and for the gel/liquid transition temperature to be above body temperature (37°C in general).

          Even more preferably, the composition according to the invention must comprise a liquid/gel transition temperature of less than 30°C and a gel/liquid  
25 transition temperature of greater than +35°C.

          Thus, the composition according to the invention is preferably a composition whose range between the liquid/gel transition temperature and the gel/liquid transition temperature is advantageously at least 20°C, the liquid/gel transition temperature preferably being between +5°C and +36°C.

30           The hydrophobic organic liquid of the composition according to the invention is a hydrophobic organic solvent or a mixture of different hydrophobic

organic solvents.

Mixtures of different hydrophobic organic solvents present the advantage to modify the gellification profile, or furthermore, to facilitate the solubilisation of some bioactives substances.

5           The hydrophobic organic solvents that may be used to prepare the composition according to the present invention belong to the group of water-immiscible organic solvents capable of creating a structure of organogel type, in the presence of a sufficient amount of "organogelling" substance as described above.

10           These solvents are preferably biocompatible, i.e. tolerated by the host organism, and trigger little or no immune reaction, for example of inflammatory or allergic type.

            Finally, it will be noted that it is preferable to use hydrophobic organic solvents that are liquid at room temperature, which simplifies the process for  
15           manufacturing and administering the composition in accordance with the invention.

            Organic solvents that can be degraded slowly, i.e. not rapidly metabolized by the enzymes present at the site of injection, and especially by lipases, will preferably be used.

20           Thus, the hydrophobic organic solvents in accordance with the invention belong to the group comprising plant oils, semi-synthetic oils and certain fatty acid esters, especially glycerol (in particular diglycerides and triglycerides).

            It may thus be envisaged to use biocompatible plant oils such as soybean oil, corn oil, cottonseed oil, groundnut oil, olive oil, castor oil, sesame  
25           oil almond oil, or cartham oil for example.

            A plant oil such as soybean oil with suitable gelling behaviour, slow biodegradability and excellent biocompatibility will preferably be used as hydrophobic organic solvent.

            Among the fatty acid esters that may be used as hydrophobic organic  
30           solvents in accordance with the invention, examples that may be mentioned especially include ethyl oleate and isopropyl myristate.

More preferably, fatty acid esters of glycerol, especially triglycerides, will be used. Even more preferably, medium-chain (fewer than 18 carbon atoms) triglycerides such as Labrafac CC<sup>®</sup>, comprising two fatty acids of 8 and 10 carbon atoms, will be used.

5        Among the synthetic or semi-synthetic solvents that may be used as hydrophobic organic solvents in accordance with the present invention, mention may be made especially of squalene, benzyl benzoate, benzyl chloride and benzyl benzoate/benzyl alcohol mixtures or Crodamol<sup>®</sup> GTCC-PN.

Synthetic hydrophobic organic oils and solvents may also be combined.

10        According to the invention, the expression "hydrophilic organic solvent" means a solvent that has high affinity for aqueous media, i.e. that is water-miscible.

The type of hydrophilic organic solvent that may be used in the present invention is advantageously a solvent capable of acting as a destabilizer for the organogel, i.e. capable of creating weak bonds with the organogelling molecules. Such a solvent is moreover advantageously biocompatible, i.e. tolerated by the body, such that its diffusion results in little or no immune reaction of inflammatory or allergic type. A solvent that has undergone approval for parenteral use will thus preferably be used for the implementation of the present invention.

20        The said hydrophilic organic solvent in accordance with the invention will advantageously be used in proportions of less than 60% by weight of the said composition, and more preferably less than 20%.

Hydrophilic solvents that may be mentioned include solvents such as alcohols, for instance ethanol, glycerol, propylene glycol, poly(ethylene) glycol of low molecular weight, benzyl alcohol or chlorobutanol, and mixtures thereof. Moreover, other water-miscible solvents may be envisaged, such as dimethyl sulphoxide (DMSO), N-methylpyrrolidone, N,N-dimethylacetamide, furfural, glycerol formal, isopropylidene glycerol, ethyl lactate, acetic acid or lactic acid, and mixtures thereof.

30        These examples are not limiting, and it may be entirely envisaged to

perform the invention using other hydrophilic organic compounds with gel-destabilizing properties, i.e. the capacity to create weak bonds with the organogelling substance in accordance with the invention.

5 The bioactive substances that may be released into the body from the organogel in accordance with the present invention are advantageously substances that are difficult to package for a sustained release, such as low molecular weight molecules of hydrophilic or very hydrophilic nature. Advantageously, the said bioactive substance will be used in proportions of from 0.5% to 70% by weight of the composition according to the invention.

10 Thus, the Applicant has tested the release from a preformed organogel of dextran molecules labelled with a fluorescent molecule: FITC (Fluoroisothiocyanate).

The release profile of the dextran was monitored *in vitro* over 20 days by assaying the fluorescence, as shown in Figure 8. The fluorescence was  
15 measured by regular sampling of an aqueous solution of phosphate-buffered saline.

Thus, the release may be designed over periods of longer than 3 days for proteins especially of therapeutic interest, such as  $\alpha$ -interferon,  $\beta$ -interferon, somatostatin, calcitonin, heparin, interleukins or erythropoietin, for peptides,  
20 amino acids or vitamins.

These examples are in no way limiting, and other types of molecules, in particular other proteins, may be entirely envisaged for such a sustained release from an organogel in accordance with the invention.

The release into the body, from the organogel according to the invention,  
25 of molecules such as certain hormones and especially certain peptide hormones such as human growth hormone, thyrotrope hormone or leuprolid, may thus be envisaged.

Thus, it may be envisaged to use the present invention for the sustained release into the body of nucleic acids, oligonucleotides or nucleic acid  
30 derivatives in particular.

Similarly, it may be entirely envisaged to perform the present invention

with the aim of dissolving and then releasing, in a sustained manner, hydrophobic bioactive substances, i.e. substances with strong affinity for the organogel and weak affinity for the surrounding aqueous medium.

The present invention may thus be used for a large number of substances of therapeutic or medical interest for which a sustained release into the body is desired.

By way of example, the composition according to the present invention may be prepared in the following manner.

10        Case of a diffusion-gelling system

The organogelling agent is first dissolved spontaneously or by heating and/or stirring in the hydrophilic organic solvent.

Next, the active substance and the hydrophobic organic solvent(s) are incorporated into this mixture, and two cases may thus be presented:

15

a) Either the active substance is soluble in the organic phase thus formed:

In this case, the active substance is dissolved in the organic phase formed. The dissolution takes place spontaneously or by heating, with or without stirring.

20

In this case, it may also be envisaged to dissolve the said active substance directly into the hydrophobic organic liquid.

b) Or the active substance is sparingly soluble or insoluble in the organic phase:

25

In this case, the active substance may first be made "wet" by dispersing it in the organic phase formed by the hydrophilic organic solvent and the organogelling substance. After stirring, a suspension of active substance in the mixture is then formed. This suspension may then be added to the other constituents of the composition according to the present invention.

30

It is also possible to dissolve the active substance in a minimum amount of water. This aqueous solution of active substance will be added to the organic phase formed by the hydrophilic organic solvent and the organogelling substance. This aqueous phase is then emulsified in the organic phase by  
5 vigorous stirring. The more vigorous the stirring, the smaller the size of the aqueous particles formed in the organic suspension and the more stable the emulsion. This emulsion can then be used for the preparation of a composition in accordance with the invention.

It should be noted, however, that this technique using an emulsion has  
10 the advantage of keeping the complex molecules of active substance in an aqueous microenvironment, which greatly limits the perturbations caused by the change of the environment, in particular possibilities of denaturing the substance.

The hydrophobic organic solvent is then added to the mixture previously  
15 obtained, optionally with stirring and/or moderate heating until a uniform mixture is obtained.

This uniform mixture according to the invention can then be injected into a living organism via the extravascular parenteral route using a conventional syringe for subcutaneous injections. After a lag phase which depends on the  
20 formulation chosen, the formation of a hardened area is observed at the site of injection, which is proof of the *in vivo* formation of the organogel according to the invention.

If it is not surgically removed, the said organogel will, depending on its size and the nature of the components constituting it, be gradually biodegraded  
25 and/or eroded in the body over a longer or shorter period. This gradual biodegradation will result in the release of the active substance that may be contained in the organogel according to the invention.

It will preferably be chosen to produce such organogels whose biodegradation will take place over periods of longer than 3 days.



Case of a cooling-gelling system

In this case, the organogelling substance with hysteresis properties is first mixed with the hydrophobic organic liquid.

5       Next, the active substance is incorporated into this mixture. If the active substance is organosoluble, it will be dissolved in the mixture directly or with gentle stirring. When the active substance is sparingly organosoluble or not organosoluble, the said substance is dispersed, as previously, in the organic phase or a stable emulsion of active substance predissolved in water is prepared, as previously, in the organic phase formed.

10       The composition thus formed is stable and preferably liquid at room temperature. It is injected, for example, via the extravascular parenteral route.

      Immediately after injection, a cold object (or any other cooling system) is held in contact with the site of injection long enough to allow the *in situ* gelation of the composition according to the present invention.

15       When the gelation is complete, the cooling system is removed. The site of injection then returns to the body temperature, the organogel according to the invention remaining stable at the said temperature.

      The heat-sensitive composition with gelling properties in accordance with the invention may be used, for example, for the delayed delivery of bioactive  
20       substances over long periods, i.e. over periods of at least one day or one week, generally more than 3 days. This composition may thus serve as a support for the delayed delivery of substances of any type, especially of substances of therapeutic or medical interest.

      It may thus be envisaged to use the heat-sensitive composition in  
25       accordance with the invention for the delayed delivery of medicinal products that need to be kept at a constant level in the blood. This invention thus proves to be particularly advantageous for medicinal products ordinarily administered several times a day and intended to maintain an effective therapeutic level in the body.

30       It may thus be envisaged to use the invention for therapeutic substances such as morphine or medicinal products that act as regulators of the

cardiovascular system or of the nervous system.

Similarly, it may be envisaged to use the composition according to the invention with the aim of overcoming certain deficiencies in the body, especially vitamin or hormone deficiencies. Thus, the present invention may serve as a support for the sustained delivery of hormones that need to be taken daily, and that are still currently administered by injection, which is a painful and restrictive mode of administration. On account of its easy administration, its harmlessness and its low cost, such a release support by organogel would eliminate these constraints for the patient.

This composition may also be used for the manufacture of a medicinal product intended to be injected into the body via the extravascular parenteral route and especially subcutaneously, intradermally, intraperitoneally or intramuscularly, intraocularly, intravascularly or vaginally, onto an open wound or during surgery.

It can, moreover, allow the manufacture of a medicinal product intended to be used as a vehicle for the sustained release of bioactive substance(s) into the body.

Figure 1 shows the diagram of the liquid-gel (solid lines) and gel-liquid (dotted lines) transition temperatures for N-lauroyl-L-alanine methyl ester (LAM) in the presence of benzyl benzoate (circles) or of a benzyl benzoate/5% benzyl alcohol mixture (triangles).

Figure 2 shows the diagram of the liquid-gel (solid lines) and gel-liquid (dotted lines) transition temperatures for LAM in the presence of soybean oil (diamonds) or Labrafac® CC (squares).

Figure 3 shows the diagram of the liquid-gel (solid lines) and gel-liquid (dotted lines) transition temperatures for N-lauroyl-L-alanine éthyl ester (LAE) in the presence of soybean oil (triangles).

Figure 4 shows the diagram of the liquid-gel (solid lines) and gel-liquid (dotted lines) transition temperatures for LAM (squares) and for N-Stearoyl-L-alanine methyl ester (SAM) (diamonds) in the presence of ethyl oleate.

Figure 5 shows the diagram of the gel-liquid transition temperatures for LAM (squares), LAE (triangles), SAM (circles), N-stearoyl-L-alanine ethyl ester (SAE) (cross) and N-lauroyl-L-alanine acid (LA) (diamonds) in corn oil.

Figure 6 and 7 shows the diagram of the gel-liquid transition temperatures for LAM (squares), LAE (triangles), SAM (circles), N-stearoyl-L-alanine ethyl ester (SAE) (cross) and N-lauroyl-L-alanine acid (LA) (diamonds) in cartham oil and crodamol® GTCC-PN (triglycerides) respectively.

Figure 8 shows the monitoring over 20 days of the *in vitro* release profile of FITC-Dextran (molecular weight = 9500) from a gel constituted with soybean oil and 30 % LAM in PBS at 37°C.

Figure 9 shows the photograph of an implant conforms to the example 5 in the injection site.

**Example 1: *In vivo* formation of an organogel from a composition in accordance with the invention**

This example seeks to confirm that the composition in accordance with the invention is indeed capable of gelling *in vivo*. The tests are performed on rats.

Soybean oil is used as hydrophobic organic solvent in accordance with the invention, and ethanol is used as hydrophilic organic solvent according to the invention.

The organogelling substance chosen is LAM (N-lauroyl-L-alanine methyl ester).

The proportions used are summarized in the following table:

Product	Function	Proportions
LAM	Organogelling agent	20% w/v
Soybean oil	Hydrophobic organic solvent	s.q. 100 mL
Ethanol	Hydrophilic organic solvent	14 % v/v

The organogelling agent is first dissolved in the ethanol. Next, the soybean oil is added to this mixture. The mixture thus obtained is stirred and heated until fully uniform. This mixture remains stable and liquid at room temperature.

5        The composition thus obtained is then injected subcutaneously. The injection is performed in the dorsal area, using a conventional syringe for subcutaneous injection. After 2 hours, the animal is sacrificed and a semi-solid gel is extracted from the site of injection, demonstrating the *in vivo* formation of the organogel.

10

**Example 2: *In vivo* formation of an organogel from a composition in accordance with the invention**

15        Soybean oil is used as hydrophobic organic solvent in accordance with the invention, and ethanol is used as hydrophilic organic solvent according to the invention.

The organogelling substance chosen is LAM (N-lauroyl-L-alanine methyl ester).

The proportions used are summarized in the following table:

20

Product	Function	Proportions
LAM	Organogelling agent	30% w/v
Soybean oil	Hydrophobic organic solvent	s.q. 100 mL
Ethanol	Hydrophilic organic solvent	18 % v/v

The injection process is identical to that of Example 1, as is the appearance of an organogel 2h 30 minutes after injection.

25

**Example 3: Manufacture of a composition according to the invention containing FITC-dextran**

This composition allows the *in vitro* measurement of the gradual release  
5 of an active substance contained in a preformed organogel.

FITC-dextran is used as active principle, which will allow, by assaying the combined fluorescence, the amount of dextran released by the organogel in accordance with the invention to be measured (cf. Figure 8).

Each point represents the mean value +/-sd (n=3). The area of gel  
10 exposed was 0.64 mm<sup>2</sup>.

Product	Function	Proportions
FITC-dextran	Active substance	1.3% w/w
LAM	Organogelling agent	30% w/v
Soybean oil	Hydrophobic organic solvent	s.q. 100 mL

The LAM is first hot-dissolved in the soybean oil. Next, the FITC-dextran is hot-dispersed in the organic phase formed, after having first ground it using a  
15 mortar, until a homogeneous liquid composition is obtained.

This liquid mixture is then introduced gelled by cooling in a test tube. An aqueous saline solution of phosphate-buffered saline is added to the gel.

Samples of the liquid surrounding the organogel in accordance with the  
20 invention are then taken over a period of 20 days. The fluorescence emitted by these samples may then be assayed and may thus confirm the sustained release of the FITC-dextran into the surrounding medium. In the event that such a gel is administered *in vivo* and in accordance with the present invention, an organic solvent of the type such as ethanol should be added so as to inhibit the  
25 gelation process before the injection.

The results of this assay are summarized in Figure 8.

**Example 4: *In vivo* demonstration of the hysteretic properties of an organogel in accordance with the invention. Example of gelation without a hydrophilic solvent.**

5           The organogelling solution is prepared from the following constituents:

Product	Function	Proportions
LAM	Organogelling agent	40% w/v
Benzylbenzoate/ 5% benzyl alcohol	Hydrophobic organic solvent	s.q. 100 mL

10           The hysteretic properties of this organogel were determined beforehand so that the liquid/gel transition temperature is less than 30°C and the gel/liquid transition temperature is greater than 37°C.

15           The organogelling solution is first brought to the liquid state by heating, and a volume of 180 µl of this solution cooled to room temperature is then injected subcutaneously into a rat. Once the injection is complete, a compress at 4°C is applied to the site of injection for 3 minutes, in order to lower the temperature thereof and to bring about gelation.

          The animal is sacrificed 2 hours 30 minutes after the injection and a visual observation of the form of the implant is made. The implant is then extracted from the site of injection and weighed.

20           In this experiment, the implant had a discoid shape about 1 cm in diameter and a weight of 130 mg.

**Example 5: *In vivo* organogel formation from a matrix consisting of a mixture of hydrophobic organic solvents.**

25           The aim of this example is to check the capacity of the organogelling agent to gellify *in vivo* an organogel consisting of a mixture of hydrophobic organic solvents. The tests are performed on rats.

          Soybean oil and ethyl oleate are used as hydrophobic organic solvents

according to the invention, and ethanol is used as hydrophilic organic solvent according to the invention.

LAM (N-lauroyl-L-alanine methyl ester) is chosen as the organogelling agent.

5 Leuprolid acetate is chosen as the bioactive substance. A leuprolid aqueous solution at 0.67 % w/v is first prepared.

The proportions of these ingredients are summarized in the following table:

Product	Fonction	Proportion
LAM	Organogelling agent	20% w/v
Ethanol	Hydrophilic organic solvent	12% v/v
Leuprolid acetate solution at 0.67 %w/v	dispersed phase containing the bioactive substance	8% v/v
Soybean oil/Ethyl oleate (50:50 v/v)	hydrophobic organic solvent	s.q. 100 mL

10

Hot dissolution of the organogelling agent in the mixture of soybean oil and ethyl oleate is first performed. Then ethanol is added to this mixture. The obtained mixture is stirred and heated until complete homogenisation. This mixture remains stable and liquid at room temperature. Leuprolid acetate is dissolved in distillate water and then added to the liquid mixture. This mixture is stirred and then emulsified with ultrasounds during two minutes.

15

Then, subcutaneous injection of the obtained composition is performed. Injection is made dorsally in rats with a conventional syringe for subcutaneous injection.

20

After two hours, the animal is sacrificed and a gel is extracted from the injection site, demonstrating the *in vivo* formation of the organogel consisting of a mixture of hydrophobic organic solvents. Figure 9 shows the form of the

implant obtained according to the composition described in this example, at the injection site.

**Example 6: Formation of an emulsion containing a bioactive substance to be included in the composition according to the present invention.**

The aim of this example is to create a stable water-in-oil emulsion (W/O), which contains a hydrophilic bioactive substance such as leuprolid in solution in the aqueous phase (dispersed phase).

Leuprolid acetate is chosen as the bioactive substance. It is dissolved in water in a 7,62 % w/v proportion.

The emulsion is stabilized with two surfactants, polysorbate 20 (Tween 20) and sorbitan trioleate (Span 85). The proportion of each surfactant is adjusted according to the hydrophilic/hydrophobic balance of the emulsion which is to be done.

The proportions of the ingredients are summarized in the following table:

Produit	Proportion (v/v)
Acetate leuprolid solution at 7,62 % w/v	12.2%
Water solution of Tween 20 at 10 % w/v	7.8%
Soybean oil solution of Span 85 at 10% w/v	2.2%
Soybean oil	77.8%

A solution at 10 % w/v Span 85 in soybean oil and a solution at 10 % w/v of Tween 20 in water are prepared. The different phases are then gathered and the mixture is stirred and heated until complete homogenisation.

This mixture remains stable and liquid at room temperature and can be



added directly to a mixture of oils, organogelling agent, and N,N-dimethylacetamide (DMAc) (see example 7).

**Example 7: *In vitro* formation of an organogel from a composition containing an emulsion and a hydrophilic organic solvent other than ethanol.**

The aim of this example is to check the capacity of a hydrophilic organic solvent other than ethanol to inhibit the gelation of the organogel at room temperature.

Soybean oil is used as a hydrophobic organic solvent and N,N-dimethylacetamide (DMAc) as a hydrophilic organic solvent.

LAM (N-lauroyl L-alanine methyl ester) is chosen as the organogelling agent

The proportions of the ingredients are summarized in the following table:

Product	Fonction	Proportion
LAM	Organogelling agent	18.4% w/v
N,N-dimethylacetamide	Hydrophilic organic solvent	18.4% v/v
W/O emulsion	Vehicle of the bioactive substance	8.2% v/v
Soybean oil	Hydrophobic organic solvent	s.q. 100 mL

Hot dissolution of the organogelling agent in soybean oil is first performed. Then DMAc is added to this mixture. The obtained mixture is stirred and heated until complete homogenisation. This mixture remains stable and is viscous at room temperature (like a cream) and can be injected as such with a conventional syringe by subcutaneous route. The gel forms subsequently to the injection of this viscous preparation.